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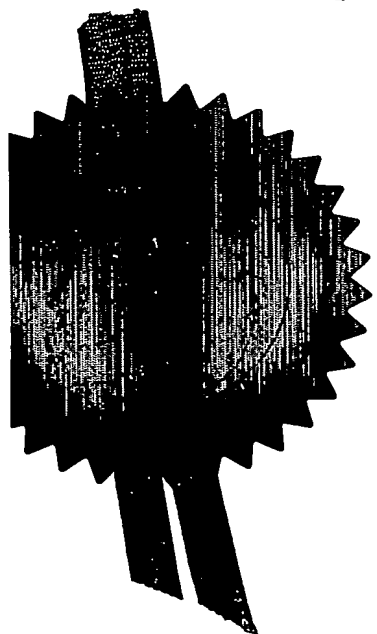
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1. Your reference 8848 GB DTD

2. Patent application number
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0228074.1

02 DEC 2002

3. Full name, address and postcode of the or of each applicant (*underline all surnames*)

Molecular Products Limited
Mill End
Thaxted
Essex CM6 2LT

Patents ADP number (*if you know it*)

6122910001

If the applicant is a corporate body, give the country/state of its incorporation

England

4. Title of the invention CARBON DIOXIDE ABSORPTION

5. Name of your agent (*if you have one*)

Abel & Imray

"Address for service" in the United Kingdom to which all correspondence should be sent (*including the postcode*)

20 Red Lion Street
London
WC1R 4PQ
United Kingdom

Patents ADP number (*if you know it*)

174001

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Country

Priority application number
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Yes

- a) any applicant named in part 3 is not an inventor, or
 - b) there is an inventor who is not named as an applicant, or
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Continuation sheets of this form

Description 8

Claim(s) 4

Abstract 1

Drawing(s) -

12

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Priority documents

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Statement of inventorship and right to grant of a patent (*Patents Form 7/77*)

Request for preliminary examination and search (*Patents Form 9/77*)

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Request for substantive examination (*Patents Form 10/77*)

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11. I/We request the grant of a patent on the basis of this application.

Signature *Abel & Imray*
Abel & Imray

Date *2nd December 2002*
2.12.02

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CARBON DIOXIDE ABSORPTION

This invention relates to a method, apparatus and device
5 for absorbing carbon dioxide from a feedstream, especially a
gaseous feedstream, more especially an air stream.

Carbon dioxide absorption is important in many fields,
especially where a person's exhaled breath is being recycled
as in certain types of underwater and emergency rescue
10 operations and, especially, anaesthesia, more especially low
flow and closed circuit anaesthesia. Chemical absorption is
frequently employed, generally using sodalime or, more
recently, enhanced formulations based on sodalime, e.g., one
using calcium or magnesium chloride to increase sodalime's
15 absorption capacity, or using an alkali metal-free
formulation, e.g., one based on calcium hydroxide and calcium
chloride. Formulations free from alkali metal hydroxides
have an advantage in anaesthesia in that they have a lower
tendency to produce toxic volatile degradation products when
20 fluorinated anaesthetics, for example sevoflurane and
desflurane, are used.

However, absorbent chemical formulations of such types
require frequent replacement, and environmentally acceptable
disposal of used materials is becoming increasingly
25 difficult.

There accordingly remains a need for a means to absorb
carbon dioxide (CO₂) that has a longer useful life. That
need must be met, however, without losing from the gas stream
and, especially, discharging to the atmosphere too great a
30 proportion of those components of the gas stream that it is
desired to retain.

There accordingly also remains a need for a means of
separating CO₂ from an anaesthetic gas-containing or similar
gas stream in which the separation factor is at an acceptable
35 level.

In this specification, the separation factor, α , is given by

$$\alpha (\text{CO}_2, a) = \frac{R_{\text{CO}_2}}{p_{\text{CO}_2}} \cdot \frac{p_a}{R_a}$$

5 wherein R represents permeation rate, p partial pressure of a gas in the feed gas stream and a an anaesthetic or other gas or gases that it is desired to retain in the feed gas stream.

There further remains a need for a means of separating
10 CO_2 from a gas stream in which variations in flow rate occur, especially the periodic flow rate variation in the gas stream from a subject under mechanical ventilation as in, for example, anaesthesia. Flow other than constant flow reduces the contact time available for reaction at the absorber
15 surface at certain periods in a cycle. If the gas transfer rate is insufficient, incomplete absorption may result unless membrane area is increased.

The present invention is based on the observation that a supported liquid membrane having certain characteristics
20 removes CO_2 from a gas stream also containing an anaesthetic at an acceptable separation factor. This has been found to be the case even when the gas stream is one in which substantial variations occur periodically in the flow rate.

The separation of CO_2 from a gas mixture using a
25 supported liquid membrane has previously been described, for example by Teramoto et al, Ind. Eng. Chem. Res. 1996, 35, 538. The membrane comprised a microporous polymer support layer and a liquid membrane phase retained in the pores of the polymer; the polymer used was poly(vinylidene fluoride)
30 and the liquid carrier was an aqueous solution of monoethanolamine or diethanolamine.

It has been found, however, that the separation factor, or membrane selectivity, of the supported liquid membranes reported by Teramoto to be good in a CO_2/CH_4 system is not
35 entirely satisfactory in a mixture of CO_2 in certain other

gases. This appears to be because the permeation rate of other gases, for example, N_2O , which should remain in the gas mixture retentate, is such that unacceptable losses through the membrane occur. Especial difficulties arise when the stream is a certain type of low flow or closed circuit anaesthetic stream.

Tests have shown that the method, apparatus, and device, of the invention are effective in separating CO_2 from a feed gas stream varying in pressure, particularly sinusoidally, as occurs in, for example, low flow or closed circuit anaesthesia, while retaining anaesthetics, e.g., N_2O and sevoflurane, to a satisfactory degree.

The invention provides apparatus for separating CO_2 from a gas stream containing CO_2 and an anaesthetic gas, the apparatus comprising a gas separation device and means for transporting the gas stream at a periodically varying flow rate through the gas separation device, the device comprising a supported carrier liquid membrane in which the carrier species is present at a concentration sufficient to provide a separation factor α (CO_2 , a), where α and a have the meanings defined above, greater than unity.

Advantageously the concentration is such as to provide an α of at least 10, preferably at least 15, more preferably at least 60, and most preferably at least 120.

One form of device capable of giving the desired separation factor, and accordingly also provided by the invention, is a device for separating gases which comprises a supported carrier liquid membrane in which the carrier species is present in a concentration of at least 4.5 mol.dm^{-3} , advantageously within the range of 4.5 to 6 mol.dm^{-3} , of liquid. The invention also provides apparatus as set out above comprising such a device.

The present invention also provides a method for the separation of carbon dioxide from a gas stream containing it,

which comprises contacting the gas stream with a supported carrier liquid membrane in which the carrier species is present in a concentration of at least 4.5 mol.dm^{-3} , advantageously within the range of from 4.5 to 6 mol.dm^{-3} , of
5 liquid.

The invention also provides a method of separating carbon dioxide from a gas stream in anaesthesia, especially low flow or closed circuit anaesthesia, which comprises contacting a gas stream containing carbon dioxide with a supported carrier liquid membrane in which the carrier is
10 present at a concentration sufficient to provide a separation factor α (CO_2 , a) as set out above. The invention further provides such a method in which the carrier is present in a concentration of at least 4.5 mol.dm^{-3} and advantageously
15 within the range of from 4.5 to 6 mol.dm^{-3} .

The gas stream advantageously passes the membrane at a periodically, e.g., sinusoidally, varying flow rate.

The means for transporting the gas stream at a periodically varying flow rate may be a bellows ventilator,
20 advantageously an air-driven, microprocessor-controlled, ventilator.

The invention further provides apparatus and a device as set out above, which also comprises means for generating a sweep gas stream, and means for humidifying the sweep stream.

25 Advantageously the carrier species is one capable of reacting reversibly with CO_2 and is soluble in or miscible with a selected solvent. The carrier species is advantageously a base, especially an organic base, for example mono-, di-, or tri-ethanolamine, diisopropanolamine,
30 ethylenediamine, or a salt of glycine, e.g., the sodium salt. As inorganic base, sodium carbonate may be given as an example. Advantageously, the solvent is one containing at least one hydroxyl group, for example one or more of glycerol, polyethylene glycol or, preferably, water. Other

organic solvents, optionally in admixture with water, may be used.

The porous membrane support may be of, for example, polypropylene, polycarbonate, poly(vinylidene fluoride), polysulphone or polyacrylonitrile. Advantageously the support is as thin as possible, consistent with a sufficient mechanical strength, and has high porosity but low pore tortuosity. When the solvent is water, the support is advantageously hydrophilic.

The membrane support may be in sheet form, for example in a spirally wound or folded sheet configuration or, preferably, in the form of hollow fibres. The fibres may typically be in the form of a bundle, which may be supported or, preferably, unsupported along its length. In order to maximize contact of gas with the fibre surfaces, the fibre packing density is as low as possible consistent with an economic size of the device. Further, in a device employing a plurality of fibre bundles, the bundles have as small a diameter as possible, and are spaced as far apart as possible, again consistent with an economic device size.

It has been found preferable for the feed stream to be within the fibres and the sweep gas to be on the shell side, this configuration enabling higher sweep gas rates to be used, maximizing CO₂ removal rates.

When a plurality of similar membrane assemblies, e.g., fibre bundles, is employed, advantageously the gas stream is divided evenly among them. Advantageously, therefore, plenum chambers are provided upstream and downstream of the membrane assemblies, enabling the gas stream to be divided and recombined.

The method of the invention may employ a vacuum on the face of the membrane remote from the gas stream; advantageously, however, a sweep gas is used to assist in transporting the permeate from the membrane surface. The

sweep gas may be, for example, ambient air, advantageously maintained at a high relative humidity. In medical and surgical uses, the air may be the supply of "medical air" normally available in hospital operating theatres, which is typically at a pressure sufficient to overcome the device resistance and the associated pressure drop. This air is, however, typically at low relative humidity, and necessitates a greater humidification capacity. When vacuum sweep is employed, lower humidification capacity but a greater capacity of vacuum plant are required.

The relative humidity of the sweep stream is advantageously maintained at a high level, preferably as close to saturation as possible, to avoid undesirable changes in the composition of the liquid membrane. Allowing or causing the carrier liquid concentration to rise above a desired level, by evaporation of solvent, especially water, may cause reduced gas transfer through the membrane by an undesirably high membrane viscosity.

Similarly, if desired or required, the feed gas stream may be humidified, by any suitable means.

The sweep gas is desirably maintained at a desired high relative humidity by, for example, delivering a metered water supply to the sweep gas stream, by a water spray or by an ultrasonic humidifier. In certain environments, condensation and recycling of moisture in the exiting sweep stream may be desirable, if health considerations permit.

Advantageously, the assembly comprises a single membrane-containing unit or a plurality of such units, especially hollow fibre membrane-containing units. Each unit advantageously contains a plurality of hollow fibres. The total surface area of the assembly is sufficient to remove enough CO_2 from an anaesthetic circuit to support life, and is advantageously in the range of 5 to 25m^3 . The surface area required may be minimized by maximizing the contact

efficiency. This may be achieved, for example, by including baffles in the shell of the assembly or by use of structured fibre packing.

The means for generating the sweep stream may be, if the stream is air, a fan or compressor capable of delivering from 7.5 to 45 litres $\text{min}^{-1} \text{m}^{-2}$, especially about 30 litres $\text{min}^{-1} \text{m}^{-2}$, of membrane area, especially about 600 l min^{-1} , through the assembly. If the sweep is a vacuum sweep, the means may be, for example, a pump capable of maintaining the shell at a pressure of at most 4mm Hg, preferably at most 0.8 mm Hg.

As indicated above, the means for humidifying the sweep stream may be, for example, a water spray or an ultrasonic humidifier.

Tests were carried out on membrane units with polyacrylonitrile fibres, surface area about 1.3 m^2 (Pan-SF 650, Asahi Medical), the fibres containing aqueous diethanolamine (DEA) solutions of various concentrations. A circuit was set up using a feed gas stream containing 23% oxygen, 77% nitrous oxide, by volume into which was fed 3% carbon dioxide, and a sweep gas stream of humidified air, all at ambient temperature. The feed gas stream was applied at a sinusoidal flow rate variation as used in mechanical ventilation of a patient under anaesthetic, at a mean flow rate of 1 litre min^{-1} , using an Aestiva 3000 unit, made by Datex-Ohmeda.

The permeation rates of CO_2 and N_2O through the membranes were measured after the concentrations of gases reached a steady state, and the results are shown in Table 1. The CO_2 concentration rate shown is an average of the "inspired" and "expired" concentrations.

Table 1

	CO ₂		N ₂ O		
DEA Concentration mol.dm ⁻³	Conc. vol %	Permeation rate ml.min ⁻¹	Conc. vol %	Permeation rate ml.min ⁻¹	α
2	1.75	39.86	28	109.44	5.83
4	1.7	39.87	37	100.66	8.62
4.5	1.8	39.73	58	73.21	17.49
5	2.0	39.55	58	73.21	15.67
5.5	1.9	39.62	62	65.38	19.77
6	2.4	39.13	61	66.35	14.99
6.5	4.2	36.15	62	60.42	8.83
7	11.2	27.88	62	47.50	3.25

α , the separation factor or membrane selectivity, is given by:

5

$$\alpha = \frac{\text{permeation rate CO}_2}{\text{partial pressure CO}_2} \times \frac{\text{partial pressure N}_2\text{O}}{\text{permeation rate N}_2\text{O}}$$

10 The final column of the table shows clearly the substantial proportional increase in desired separation of CO₂ over unwanted loss of N₂O between 4 and 4.5 mol.dm⁻³ concentrations, this being maintained almost to the highest concentration tested. The example above shows that the

15 carrier species at the concentrations used readily gives an α of from 15 to 20 under the test conditions. However, as can be seen from the second column of the table, the CO₂ permeation rate and α value begin to fall when the concentration exceeds about 6 mol.dm⁻³.

20 It is believed that an optimum concentration is equivalent to that in which the amine is substantially fully hydrated with little or no greater proportion of solvent e.g., water.

CLAIMS:

1. Apparatus for separating CO₂ from a gas stream containing CO₂ and an anaesthetic gas, the apparatus comprising a gas separation device and means for transporting the gas stream at a periodically varying flow rate through the gas separation device, the device comprising a supported carrier liquid membrane in which the carrier species is present at a concentration sufficient to provide a separation factor α (CO₂, a),

$$\text{where } \alpha (\text{CO}_2, a) = \frac{R_{\text{CO}_2}}{p_{\text{CO}_2}} \cdot \frac{p_a}{R_a}$$

wherein R represents permeation rate, p partial pressure of a gas in the feed gas stream and a an anaesthetic gas, greater than unity.

2. Apparatus as claimed in claim 1, wherein the carrier species concentration is such as to provide an α value of at least 15.
3. Apparatus as claimed in claim 2, wherein the α value is at least 60.
4. Apparatus as claimed in any preceding claim, wherein the device comprises a supported carrier liquid membrane in which the carrier is present in a concentration of at least 4.5 mol.dm⁻³.
5. Apparatus as claimed in claim 4, wherein the carrier is present in a concentration within the range of from 4.5 to 6 mol.dm⁻³.
6. Apparatus as claimed in any preceding claim, wherein the carrier comprises an organic base.

7. Apparatus as claimed in claim 6, wherein the base is diethanolamine.

5 8. Apparatus as claimed in any preceding claim, wherein the carrier liquid is an aqueous solution.

9. Apparatus as claimed in any one of claims 1 to 7, wherein the carrier liquid is a solution of the carrier in an
10 organic solvent.

10. Apparatus as claimed in any preceding claim, wherein the membrane support is a porous polymer.

15 11. Apparatus as claimed in claim 10, wherein the polymer is a polysulphone or polyacrylonitrile.

12. Apparatus as claimed in any preceding claim, wherein the membrane is a hollow fibre membrane.

20

13. Apparatus as claimed in claim 12, wherein the membrane is in the form of a fibre bundle.

14. Apparatus as claimed in any preceding claim, which also
25 comprises means for generating a sweep gas stream.

15. Apparatus as claimed in claim 14, which comprises means for humidifying the sweep gas stream.

30 16. A device for separating gases which comprises a supported carrier liquid membrane in which the carrier is present in a concentration of at least 4.5 mol.dm^{-3} .

17. A device as claimed in claim 16, wherein the carrier is present in a concentration within the range of from 4.5 to 6 mol.dm⁻³.

5 18. A device as claimed in claim 16 or claim 17, wherein the carrier comprises an organic base.

19. A device as claimed in claim 18, wherein the base is diethanolamine.

10

20. A device as claimed in any one of claims 16 to 19, wherein the carrier liquid is an aqueous solution.

21. A device as claimed in any one of claims 16 to 20,
15 wherein the membrane support is a porous polymer.

22. A device as claimed in claim 21, wherein the polymer is a polysulphone or polyacrylonitrile.

20 23. A device as claimed in any one of claims 16 to 22, wherein the membrane support is in the form of a hollow fibre.

24. A device as claimed in claim 23, wherein the membrane
25 support is in the form of a fibre bundle.

25. A device as claimed in any one of claims 16 to 22, wherein the membrane support is in sheet form.

30 26. A device for separating carbon dioxide from a gas stream containing carbon dioxide and an anaesthetic gas, which device comprises a supported carrier liquid membrane assembly in which the carrier is present in a concentration of at least 4.5 mol.dm⁻³.

35

27. A device as claimed in claim 26 having one or more of the features defined in any of claims 17 to 25.

28. A method of separating carbon dioxide from a gas stream
5 in anaesthesia, which comprises contacting the gas stream with a supported carrier liquid membrane in which the carrier is present in a concentration of at least 4.5 mol.dm⁻³.

10 29. A method of separating carbon dioxide from a gas stream in anaesthesia, which comprises contacting the gas stream with a supported carrier liquid membrane in which the carrier is present at a concentration sufficient to provide a separation factor α (CO₂, a) of at least unity.

15

30. A method as claimed in claim 29, wherein the carrier is present at a concentration sufficient to provide a separation factor of at least 15.

20 31. A method as claimed in claim 29, wherein the carrier is present at a concentration sufficient to provide a separation factor of at least 60.

32. A method as claimed in claim 29, wherein the carrier is
25 present in a concentration of at least 4.5 mol.dm⁻³.

33. A method as claimed in any one of claims 28 to 32, wherein the carrier is as defined in any one of claims 5 to 9.

30

34. A method for the separation of carbon dioxide from a gas stream containing it, which comprises contacting the gas stream with a supported carrier liquid membrane in which the carrier is present in a concentration of at least 4.5

35 mol.dm⁻³.

CARBON DIOXIDE ABSORPTION

ABSTRACT

5

Carbon dioxide is separated from a gas stream using a supported carrier liquid membrane having a selected concentration of carrier species, the method being especially suitable for use in anaesthesia under conditions of periodic
10 flow.